

IN THE SPECIFICATION:

Page 10, second paragraph:

The Insertion Tube, which makes up the rest of the 60-150 cm length, is not capable of controlled deflection. It has a tailored bending flexibility and torque transmission which is of major importance in endoscope design. Most instruments have two-stage bending stiffness, i.e., the distal portion of the insertion tube is more flexible than the proximal portion. The flexibility flexibility of each portion of the insertion tube requires extensive clinical testing to ensure that the endoscope handles easily and produces a minimum of patient discomfort.

Page 26, first full paragraph:

The diameter of the helix formed by thread 103 of catheter 101 is referred to as thread diameter 103d, and is equal to two thread heights 103b plus the outside diameter 102d of catheter tube 102, or in this case 2 times 0.032 inches plus 0.125 inches or approximately 0.19 inches. The circumference C of the helix formed by thread 30 103 is calculated as π (pi) times thread

diameter 103d, or in this case 3.14 times 0.19 or approximately 0.6 inches.

Page 26, last paragraph, continuing onto page 27:

Both ends of thread 103 are tapered from zero to full height in one-half turn of the helix, to facilitate gentle, gradual displacement of urethra wall 002 by thread 103 when catheter 101 is rotated clockwise for advancement into the urethra and counterclockwise for retraction. The difference between thread width ~~103b~~ 103a and pitch 103c shown in FIG. 3 is sufficient that the urethra wall 002 does not bridge between adjacent turns of thread 103, but rather is only displaced in a manner closely conforming to the cross section of thread 103, thereby providing the longitudinal grip on urethra wall 002 for advancing and retracting the catheter.

Page 28, first paragraph:

Referring to FIGS. 5 and 6, thread 113 of catheter 111 is formed from a strip of polyurethane material with a rectangular cross section of width 113a of 0.05 inches and height ~~31b~~ 113b of

0.10 inches, attached to tube 112 starting 0.2 inches from distal end 115 and extending four turns around tube 112 in a clockwise direction towards proximal end 116 at a uniform pitch 113c of 0.25 inches, resulting in a four-turn thread or helix about one inch long.

Page 32, first full paragraph:

Referring now to FIGS. 16-18, a threaded urethral stent 301 made from polyurethane material has a tube 302 with an external thread 303 of uniform pitch. Thread 303 is similar to thread 103 on catheter 101 of FIGS. 2 and 3, wherein the height of the thread is at least twenty percent (20%) of the diameter of the shaft 202 102, and the ratio of thread pitch to the circumference of the thread diameter is less than one to one (1/1). The ends of thread 303 are tapered for ease of advancing and retracting through a passage. There is an interior shoulder 304 at the distal end 305 of the stent, and a bushing 307 of relatively harder material with a tapered interior wall 308 extending from the bushing's full diameter at one end to a uniform hexagonal aperture 309, bushing 307 being affixed within the proximal end 306 of the stent and oriented with tapered wall 308 extending

proximally from aperture 309. Coiled sidewall reinforcement member 310 is secured within the remaining length of stent 301 by bushing 307 and interior shoulder 304. Alternative embodiments may have a section of the thread being tapered to a lesser height or no height, to provide a "waist" for gripping by a muscular zone such as the prostate or sphincter. Also, reinforcement member 310 could be configured or molded into the sidewall tube 302.

Page 34, first full paragraph:

There is an interior shoulder 364 at the distal end 365 of catheter 361, a bushing 367 of relatively harder material with a tapered interior wall 368 extending from the bushing's full diameter at one end to a uniform hexagonal aperture 369, bushing 367 being affixed within the ~~distal proximal~~ end 366 of catheter 361 and oriented with tapered wall 368 extending proximally.

Page 34, third full paragraph:

Referring to FIGS. 19, 21, 23 and 24, alternate hexagonal tip 384 for stylet 331 has a slightly concave proximal end 385

and flutes 386. When used in conjunction with stent-follower 341 to actuate the check valve of catheter 361, tip 3 84 is be inserted through aperture 369 of catheter 361 to push ball 371 upward against coil member 370, thereby opening the check valve function and permitting outward flow of fluid through flutes 386 and aperture 369 into and through stent-follower 341.

Page 34, last paragraph:

Referring now to FIGS. and 25-29, the threaded suprapubic catheter 401 of FIGS. 25 and 26 is constructed with a flexible tube 402 with a lumen 408 connecting axial ports at the proximal end and the distal end, and an external thread 403 of uniform pitch applied at it's distal end. As described for catheter 101 of FIG. 2 and 3, the ratio of thread pitch 403c to the circumference of thread diameter 403d is much less than one to one (1/1). Tube 402 is of sufficient torsional strength to accept and transmit rotational finger force applied at the proximal end to the distal end. The ends of thread 403 are tapered for ease of advancing and retracting the catheter through the abdomen and into the bladder wall.

Page 37, third paragraph:

Referring to FIG. 33, camera assembly 520 is shown installed in camera introducer catheter 501 500, with camera 521 secured within tip 501 by set screw 512, so that the camera views forward through the window. The camera assembly and catheter are combined here as a camera introducer system.

Page 37, fourth paragraph:

Referring to FIG. 34, rotating container and dispensing system 550 consists of drum 551 with axial opening 552 around which handle 553 is rotatably attached. Catheter 501 500 is rotatingly dispensed during application by holding handle 553 and rotating drum 551 while catheter 401 500 is being rotatingly advanced in the subject colon.